Photosensitizers

Photodynamic Therapy Efficacy Enhanced by Dynamics: The Role of Charge Transfer and Photostability in the Selection of Photosensitizers

Luis G. Arnaut, *^[a, b] Mariette M. Pereira,^[a] Janusz M. Dabrowski, *^[c] Elsa F. F. Silva,^[a] Fábio A. Schaberle,^[b] Artur R. Abreu,^[b] Luís B. Rocha,^[d] Madalina M. Barsan,^[a] Krystyna Urbańska,^[e] Grażyna Stochel,^[c] and Christopher M. A. Brett^[a]

Abstract: Progress in the photodynamic therapy (PDT) of cancer should benefit from a rationale to predict the most efficient of a series of photosensitizers that strongly absorb light in the phototherapeutic window (650–800 nm) and effi $ciently$ generate reactive oxygen species (ROS=singlet oxygen and oxygen-centered radicals). We show that the ratios between the triplet photosensitizer– $O₂$ interaction rate constant (k_D) and the photosensitizer decomposition rate constant (k_d), k_D/k_d , determine the relative photodynamic activities of photosensitizers against various cancer cells. The same efficacy trend is observed in vivo with DBA/2 mice bearing S91 melanoma tumors. The PDT efficacy intimately depends on the dynamics of photosensitizer–oxygen interactions: charge transfer to molecular oxygen with generation of both singlet oxygen and superoxide ion (high k_D) must be tempered by photostability (low k_d). These properties depend on the oxidation potential of the photosensitizer and are suitably combined in a new fluorinated sulfonamide bacteriochlorin, motivated by the rationale.

Introduction

Photodynamic therapy (PDT) combines light, a photosensitizer, and oxygen to generate reactive oxygen species (ROS: singlet oxygen and oxygen-centered radicals) and destroy targeted tissue.^[1] PDT is progressively becoming a credible alternative to surgery, chemotherapy, and radiotherapy in the management of cancer because it can be repeated many times in the same site and has no long-term side effects.^[2] The directionality of laser light, the eventual affinity of photosensitizers to-

wards tumors, and the short diffusion radius of the ROS minimize damage to healthy tissues. Moreover, the oxidative stress induced by these ROS triggers the local destruction of the tumor, whereas the local inflammation resulting from PDT activates antitumor immune responses capable of causing regression in distant tumors and induce long-term immune memory.^[3] Although a handful of photosensitizers are currently used for various indications, $[4]$ the realization of the full potential of PDT still awaits the development of more efficient photosensitizers with reduced skin photosensitivity after treatment.

Various authors have discussed photosensitizer properties critical to the success of PDT. $[5]$ Generally accepted properties are low dark toxicity, amphiphilicity, selectivity towards tumor tissue, simple formulation, long shelf-life, rapid clearance from the body, facile synthesis, feasible scaleup, 700 nm $< \lambda_{\text{max}}$ 800 nm, $\varepsilon_{\sf infrared}$ $>$ 10⁵ m⁻¹ cm⁻¹, $\varPhi_{\sf F}$ \geq 0.2, $\varPhi_{\sf T}$ \geq 0.7, triplet lifetime $\tau_{\text{\tiny T}}$ \geq 100 µs, \varPhi_{Δ} $>$ 0.5, and \varPhi_{pd} $<$ 10⁻⁵, in which \varPhi refers to quantum yields of fluorescence (F), triplet (T), singlet oxygen (Δ) , and photodecomposition (pd). Singlet oxygen is generated by energy transfer from the photosensitizer triplet state to molecular oxygen (type II reaction), but the triplet state of the photosensitizer may also participate in electron or hydrogenatom transfer reactions (type I reaction) that eventually lead to oxygen-centered radicals.^[6] Interestingly, charge-transfer interactions between the triplet state of the photosensitizer and molecular oxygen facilitate the generation of the superoxide ion and the hydroxyl radical, in addition to singlet oxygen, and increase phototoxicity.^[5e, 7] Moreover, the localization of the

In the corresponding chlorins (e.g., $mTHPC$ or Foscan), one $\overline{\cdots}$ is a single bond and the other is a double bond.

Scheme 1. Promising bacteriochlorin photosensitizers and the general structures of photosensitizers discussed in this study.

photosensitizer in the endoplasmic reticulum (ER) and its ability to generate strong ROS-dependent ER stress was shown to induce immunogenic cancer cell death.^[8]

Current efforts to make the "ideal photosensitizer" focus on bacteriochlorins because they intrinsically have some of the desired properties mentioned above.[9] Scheme 1 illustrates bacteriochlorins currently investigated and our own halogenated tetraphenylbacteriochlorins.^[10] The use of naturally occurring bacterichlorins, or their derivatives such as WST11, is very appealing and substantiated by interesting results, $[11]$ but their (photo and thermal) stability is less than ideal. Alternatively, de novo synthesis of more stable bacteriochlorins such as $(NC)_2B-Pd$ is now a well-established multistep route capable of generating a wide range of bacteriochlorins with tunable properties.^[12] Our focus on halogenated tetraphenylbacteriochlorins was motivated by the ability to synthesize a wide variety of porphyrin precursors in two to three steps followed by the one-step reduction to the corresponding bacteriochlorin in the absence of solvents, $[10, 13]$ and by their stability, $[10, 14]$ strong absorption in the near-infrared region, efficient generation of ROS,^[15] ER localization, and favorable biodistribution.^[7,16]

Access to a vast library of compounds with therapeutic potential is a critical step in the discovery of new drugs. However, the potential of the therapy can only be fully exploited with a rationale that uses observable properties to anticipate the best drug candidate. Structure–activity relationships have been notoriously difficult to establish for PDT photosensitizers. Hamblin, Lindsey, and co-workers reported that 10 J cm⁻² at 732 nm required 0.1 µm of a bacteriochlorin with $log P_{OW} = 2.3$ to kill 50% of HeLa cells but a related bacteriochlorin with $log P_{\text{OW}} = 1.4$ required 4 μ m.^[9c] Pandey and co-workers provided examples of phototoxicities of ketobacteriochlorins towards Colon26 cells differing by more than one order of magnitude with subtle changes in structure.^[17] We also showed that the photodynamic effect in vitro is not simply correlated with any of the properties judged critical to the success of PDT, $^{[7]}$ and that tumor growth delays in animal models are very sensitive to subtle changes in properties (27 days for CIBOH^[16b] to 44 days for $CI₂BEt$).^[16c] This work discloses illuminating dependences of PDT efficacy on the dynamics of the charge transfer between the photosensitizer and oxygen (which determine the nature of the ROS generated), and on the stability of the photosensitizer (which determines its throughput). These dependences are expected to be ubiquitous phenomena affecting the performance of all photosensitizers and provide the grounds to pre-

dict the most efficient of a family of photosensitizers. The rationale derived by these dependences motivated the detailed investigation of a new fluorinated sulfonamide bacteriochlorin for PDT of cancer (F₂BMet, Scheme 1).

Results

Synthesis

The synthesis was oriented by the requirements of simplicity, feasibility of scaleup, and ability to offer a variety of stable bacteriochlorins. The synthesis of ortho-halogenated phenyl porphyrins using the nitrobenzene method,^[18] with the modulation of their amphiphilicity by means of chlorosulfonation followed by reaction with nucleophiles,^[19] led to the desired halogenated sulfonamide porphyrins.^[20] We selected the solventfree diimide hydrogenation method (Scheme 2) to obtain the bacteriochlorins in view of its simplicity and functional-group tolerance.^[13] Details of the synthesis are given in the Experimental Section.

Photophysics and photochemistry

Table 1 presents the absorption, fluorescence, and triplet properties of tetraphenylporphyrin derivatives and Photofrin (a mixture of hematoporphyrin derivatives for injection, approved for clinical use) taken from the literature, and new data on F_2 PMet and F_2 BMet. F_2 BMet was synthesized in this work to meet the requirements of photostability and large charge-transfer interactions with oxygen. F₂BMet has ε_{743} = 140 000 m⁻¹ cm⁻¹ in ethanol (Figure 1) and the Beer–Lambert law is followed in the micromolar range. The molar absorption coefficient is based on the chromatographic content of the sample and it is larger

Scheme 2. One-step synthesis of F_2 BMet from F_2 PMet without using solvents or bases.

than those of related bacteriochlorins in Table 1 (e.g., CI_2BEt) because earlier corrections only accounted for chlorin impurities.^[10] However, this ε_{743} is in excellent agreement with those of halogenated tetraphenylbacteriochlorins purified by preparative thin-layer chromatography.^[14a]

The fluorescence quantum yield of chlorinated tetraphenylbacteriochlorins is very low (Cl₂BEt, Φ _F=0.013),^[23a] as expected from the internal heavy-atom effect,^[21b] but the analogous fluorinated bacteriochlorin has an intense fluorescence (F_2 BMet, $\Phi_{\rm F}$ = 0.138 \pm 0.011) that may provide guidance for the location of the tumor tissue during therapy. The Supporting Information presents the 3.0 ns fluorescence decay at 765 nm measured by single-photon counting with excitation at 378 nm, and its fitting to a monoexponential function.

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Figure 1 also presents the transient absorption spectrum and decays of solutions of F2BMet in ethanol. The monoexponential decays give triplet life-

times of τ_{T}^0 = 47 µs and τ_{T} = 216 or 50 ns in nitrogen-, air-, or oxygen-saturated solutions, respectively. The bleaching of the ground-state absorption of F2BMet at 745 nm recovers almost quantitatively and was used to calculate the triplet molar absorption coefficient at 790 nm $(\varepsilon_T = 55000 \text{ m}^{-1} \text{ cm}^{-1})$, which was then used to obtain the triplet quantum yield, Φ _T=0.65 \pm 0.10, by employing benzophenone as reference.

Time-resolved photoacoustic calorimetry (PAC)^[15,21a] was used to measure the heat released after pulsed-laser excitation of the bacteriochlorin. Deconvolution of the PAC signals using

Table 1. Data for halogenated sulfonamide porphyrin derivatives in ethanol or methanol, and of halogenated porphyrin derivatives in toluene, compared with those of tetra(3-hydroxyphenyl)porphyrin derivatives and Photofrin, and photodegradation in PBS/methanol.

[a] Oxidations assigned to PhSO₂NHR or PhSO₃H groups; E_{red} $=-0.27$ V found for F₂BOH is also assigned to the PhSO₃H group. [b] Refs. [14a, 18, 21], with oxidation potentials in CH₂Cl₂ and reduction potentials in DMF vs SCE from Ref. [22]. [c] Partly from Refs. [7, 10, 15, 23]. [d] Oxidation potentials in benzonitrile in Ref. [24] corrected for the difference of oxidation potentials for that study and in Ref. [22]. [e] Partly from Refs. [20, 25]. [f] From Ref. [26]. [g] In H₂O/ MeOH, 2:3 v/v. [h] In PBS, but for CIBOH $\varPhi_{\rm pd}$ changes only from 2.8×10⁻⁴ in PBS to 3.0×10⁻⁴ in PBS/MeOH. [i] In methanol from Refs. [27,28]. [j] \varPhi_{Δ} refers to 10 μm hematoporphyrin derivative in PBS (Ref. [29]).

Figure 1. F_2 BMet absorption (solid line, 6.5 μ m) and fluorescence (dotted line, λ_{max} = 735 nm) and transient absorption (line and circles, collected 30 ns after the laser pulse) in ethanol. Inset: decays at 780 nm in nitrogen-, air-, or oxygen-saturated ethanol measured by laser flash photolysis at 20 \degree C with λ_{exc} = 355 nm.

a photoacoustic reference gives the energy released first in the formation of the triplet and then in the decay of the triplet.^[30] The fast heat released was used together with Φ _T=0.65 \pm 0.10 to obtain the triplet-state energy of F₂BMet as $E_T=(26\pm2)$ kcal mol⁻¹. The second heat release in the presence of oxygen was used together with the energy and quantum yield of singlet oxygen to obtain the energy stored in other ROS, $\Phi_{\text{CT}}E_{\text{CT}}=$ (4.5 ± 0.6) kcalmol⁻¹, in which E_{CT} is the energy of the chargeseparated state generated by electron transfer from F_2 BMet to molecular oxygen and Φ_{CT} is the corresponding quantum yield. Details are given in the Supporting Information.

Reactive oxygen species

Excitation of bacteriochlorins at 355 nm in ethanol generates singlet oxygen with its characteristic phosphorescence at 1270 nm with a lifetime of approximately 14 µs. The singlet-oxygen quantum yields were obtained by using the phosphorescence intensities according to a previously described procedure.^[15] Representative data are presented in the Supporting Information. Evidence for the photogeneration of other ROS, such as O_2 ⁻ and OH', has been obtained in DMSO and phosphate-buffered saline (PBS) solution using 5,5-dimethyl-1-pyrroline N-oxide (DMPO) as spin trap to form DMPO-OOH and DMPO-OH radical adducts

while irradiating bacteriochlorins, and EPR to identify such adducts.[15] The Supporting Information presents similar evidence obtained with the irradiation of F_2 BMet. In the presence of 30 μ g mL⁻¹ catalase or of 50 μ g mL⁻¹ superoxide dismutase, the DMPO-OH signal disappeared completely. These findings corroborate our mechanism of hydroxyl radical formation in aqueous solution as a sequence of steps involving the superoxide ion and hydrogen peroxide.^[15] Moreover, after the addition of NaN₃ (5 mm), a singlet-oxygen inhibitor, we still observe the DMPO-OH EPR signal, which indicates that singlet oxygen is not involved in the formation of OH⁺ by F₂BMet.

Electrochemistry

Cyclic voltammograms were recorded at slow sweep rates, 25 mV s^{-1} , in acetonitrile or dichloroethane containing 0.1 M tetra-n-butylammonium perchlorate. Figure 2 presents typical cyclic voltammetric responses of sulfonamide porphyrin derivatives. Table 1 lists the lowest redox potentials measured in this work. E_{red1} and E_{ext} refer to the macrocycle and E_{ext} to the sulfonic or sulfonamide groups.

The bacteriochlorins investigated, excepting F_2BOH , undergo two reversible reductions at $E_{\text{red1}} = -0.74$ to -0.95 V versus a saturated calomel electrode (SCE) and $E_{red2} = -1.15$ to -1.46 V versus SCE, respectively, to form the radical anion and dianion. Two reversible oxidations were also recorded at $E_{ox1}=$ 0.65–0.82 V versus SCE and E_{ox2} = 1.18–1.24 V versus SCE, which correspond to the formation of the radical cation and dication. The first oxidation is reversible, whereas the second one is quasi-reversible or irreversible owing to the instability of the dication generated.^[31] F₂BOH presents three irreversible oxidations, the third one occurring at a less positive potential of $+0.55$ V and the corresponding reduction at -0.27 V versus SCE, which correlated with the oxidation and reduction of the Ph-SO₃H group.

The presence of the sulfonamide electron-withdrawing group in the phenyl ring increases the first oxidation potential

Figure 2. Left panel: cyclic voltammogram recorded in 0.1 m TBAP dissolved in CH₃CN containing 0.5 mm F₂BMet; scan rate 25 mV s⁻¹. Right panel: cyclic voltammogram recorded in 0.1 m TBAP dissolved in CH₃CN containing 0.5 mm Cl₂PEt; scan rate 25 mV s⁻¹.

from $+0.65$ in F₂B to $+0.80$ in F₂BMet and to $+0.82$ in Cl₂BEt. Cl₂PEt and Cl₂CEt exhibited similar cyclic voltammetric responses, characterized by two reversible reductions and three oxidations. The third oxidation wave at less positive potentials, of approximately $+0.85$ V versus SCE, is related to irreversible sulfonamide oxidation, visible in the case of porphyrins and chlorins, in which the first oxidation of the macrocycle occurs at more positive potentials, $+1.38$ and $+1.36$ V versus SCE, for Cl₂PEt and Cl₂CEt, respectively. Similar oxidation potential values corresponding to sulfonamide have been reported for sulfadiazine^[32] and sulfaguanidine.^[33] The oxidation of the sulfonamide group overlaps with the first oxidation of the macrocycle, located at $+0.80$ and $+0.82$ V versus SCE for F₂BMet and $Cl₂BEt$, respectively. CIPOH, which contains the same $-SO₃H$ group as F2BOH, presents three irreversible oxidation processes, with the less positive potential being $-SO_3H$ oxidation, at $+$ 0.70 V versus SCE. The oxidation of the $-$ SO₃H group occurs at lower potentials than that of the sulfonamide $-SO_2$ NHR group.

The potential difference, ΔE , between the first oxidation and first reduction couples, $\Delta E_{\text{o}x1-{\text{red1}}},$ decreases in the order porphyrin>chlorins>bacteriochlorins, with values of 2.32, 2.20, and approximately 1.57 V versus SCE, respectively. The assignment of the oxidation and reduction potentials is consistent by the correlation between $E_{\text{ox1}}^0 - E_{\text{red1}}^0$ and the singlet-state energy (E_s) of these macrocycles.^[9d]

The energy of the full electron transfer from the photosensitizer to molecular oxygen is given by $\Delta G_{\text{CT}}\!=\!E_{\text{ox}}^*\!-\!E_{\text{red}}^{\text{A}}$ in which E_{ox}^* = E_{ox1}^D – E_T is the triplet-state oxidation potential, and the half-wave reduction potential of oxygen is $E_{\text{red}}^{\text{A}}$ = -0.78 V versus SCE in DMSO,^[34] or -0.425 V versus SCE in hydrogenbonding solvents.[35] This latter value is more relevant for biological reactions and for the determination of ΔG_{CT} in ethanol. The ΔG_{CT} values used in this work were calculated with $\mathit{E}^{\text{A}}_{\text{red}}$ $=$ -0.425 V versus SCE. For F₂BMet we calculate $\Delta G_{CT} = (2 \pm 1)$ 2) kcal $\,$ mol $^{-1}$ (ΔE_{CT} $=$ 28.2 kcal $\,$ mol $^{-1}$ and $\,\varPhi_{\text{CT}}$ $=$ 0.16 \pm 0.02).

$$
v_{\rm d} = \frac{\mathrm{d}n}{\mathrm{d}t} = \frac{V_{\rm irr} N_{\rm A}}{\varepsilon l} \frac{\mathrm{d}A}{\mathrm{d}t} = k_{\rm d}[S] \tag{2}
$$

$$
v_{\rm p} = \frac{\lambda P}{hc} (1 - 10^{-A}) \tag{3}
$$

and k_d is the decomposition rate constant, P the power of the monochromatic incident light absorbed in the volume (V_{irr}) by a solution of absorbance A. Table 1 shows published Φ_{nd} values of some halogenated bacteriochlorins,^[10] together with additional data obtained in aerated solvents for F₂BMet (laser irradiation at 748 nm) and for halogenated sulfonamide porphyrins and chlorins (pulsed-laser excitation at 508 or 653 nm, respectively). The similar Φ_{pd} values of Cl₂PEt, Cl₂CEt, and Cl₂BEt is readily explained in terms of their lowest oxidation potentials. The irreversible oxidation of the sulfonamide group and reversible oxidation of the bacteriochlorin macrocycle, which occur at very similar oxidation potentials, control the decomposition rate.

Free-energy relationships

The triplet-state quenching rate constant is given by Equation (4):

$$
k_{\rm q} = (1/\tau_{\rm T} - 1/\tau_{\rm T}^{0})/[O_{2}] \tag{4}
$$

but residual oxygen in N_2 -saturated solutions leads to underestimates of τ_{τ}^0 in organic solvents in which $\tau_{\tau}^0 > 30$ µs. In such cases, it is more appropriate to calculate the triplet-state quenching rate constant as $k_{0}=1/(\tau_{\text{T}}[O_{2}])$. The rate constants presented in Table 1 were calculated with this equation and the concentration of oxygen in the solvent of the experiment. Figure 3 presents the dependence of k_q on ΔG_{CT} and of Φ_{pd} on the lowest E_{ox} . The $E_{\text{ox}1}$ of THPP, THPC, and THPB were taken from TPP, TPC, and TPB, respectively.

In the absence of charge transfer in the {sensitizer \cdots O₂} encounter complex, spin statistics limit k_a to one ninth of the diffusion rate constant ($k_{\text{diff}} = 9.5 \times 10^9 \text{ m}^{-1} \text{ s}^{-1}$ in ethanol).^[23b] How-

Photodecomposition

The photostability of a photosensitizer (S) is best described by its photodecomposition quantum yield (Φ_{pd}) , which is defined as the ratio between the rate of disappearance of photosensitizer molecules and the rate of absorption of photons as shown in Equation (1):

$$
\varPhi_{\text{pd}} = v_{\text{d}}/v_{\text{p}} \tag{1}
$$

in which v_d and v_p are defined by Equations (2) and (3), respectively:

ever, the rate constant of charge-transfer-assisted quenching of porphyrin derivatives by molecular oxygen increases with the free energy of the reaction and should approach $^{4}/_{9}$ $k_{\sf diff.}$ $^{15,36]}$ Bacteriochlorins show $k_{\sf q}\!>\!{}^1\!/_9$ $k_{\sf diff}$ and $\varPhi_{\Delta}\!<$ 1, which are the hallmarks of charge-transfer interactions between a photosensitizer and molecular oxygen.^[15,37] Thus, the dependence of k_a on ΔG_{CT} can be regarded as a free-energy relationship. In hydrogen-bonding solvents, the $-\Delta G_{\textrm{CT}}$ driven charge-transfer dynamics increase the formation of superoxide ion. FBMet, F₂BMet, ClBEt, and mTHPB exhibit $k_q > 2 \times$ 10^9 M^{-1} s⁻¹ and are good examples of photosensitizers that take advantage of this effect.

 $\Phi_{\rm{nd}}$ is a measure of the decomposition rate constant ($k_{\rm{d}}$) under constant power of absorbed light (P). The photodecomposition products of bacteriochlorins and chlorins are oxidation products and, therefore, the dependence of Φ_{nd} (or k_{d}) on E_{ox} is also a free-energy relationship. The condition of photostability (\varPhi_pd $<$ 10⁻⁵) requires E_ox $>$ 0.7 V versus SCE, which is met by F_2 BMet and Cl₂BEt in Table 1.

These two free-energy relationships show that strong charge transfer to molecular oxygen (high k_q) and high photostability (low Φ_{nd}) are singularly combined in F₂BMet. It should be emphasized that the solubility of oxygen decreases from organic solvents ([O₂]_{ethanol} = 2.1 mm, $[O_2]_{\text{toluene}} = 1.8$ mm)^[38] to water $([O_2]_{aa} = 0.29$ mm at 20 °C), and that the oxygen partial pressure decreases from $pO₂=150$ mm Hg for cell cultures to 14 mm Hg in the blood vessels and to 5 mm Hg some $70-80 \mu m$ away from the closest blood vessel.^[39] Thus, the kinetics of the interaction between the photosensitizer triplet state and oxygen assumes an even greater relevance in vivo. The photobleaching of photosensitizers in biological media is also severe, and we can expect the high k_q and low Φ_{pd} of F₂BMet to be most valuable for PDT. This motivated additional work to characterize the biological activity of F_2 BMet.

In vitro studies

Intracellular localization was investigated in A549 cells co-incubated with F_2 BMet and fluorescent probes specific for lysosomes, mitochondria, or endoplasmic reticulum. Figure 4 shows the overlaid images, with the fluorescence of F_2 BMet in red and that of the organelle-specific probes in green. The topographic profiles of F_2 BMet reveal a high degree of localization in the ER, some in the mitochondria, and none in the lysosomes, which is consistent with those of other halogenated sulfonamide bacteriochlorins.^[7]

 F_2 BMet was also co-incubated with 3'-(p-aminophenyl)fluorescein (APF), because this probe reacts rather selectively with the hydroxyl radical to release fluorescein that has a characteristic fluorescence near 520 nm.^[40] Figure 5 shows the fluorescence of F₂BMet in cells and the fluorescence of fluorescein observed after the illumination of one cell at 514 nm with the argon laser of the confocal microscope. The argon laser was controlled to illuminate only one cell, and only this cell showed fluorescein emission. The OH' radical formed upon illumination of F_2 BMet in vitro reacts locally with APF and leads to the fluorescein emission. The Supporting Information presents the case of the illumination of the whole cell culture with a diode laser at 750 nm.

Photocytotoxicity

Incubation of A549 and S91-I3 cells for 20 h with F_2 BMet in the 0.5-25 µm concentration range, or of CT26 and HT-29 with up

Figure 4. Fluorescence micrographs of A549 cells showing intracellular localization of F₂BMet evaluated by confocal microscopy. Cells were marked with dyes for endoplasmic reticulum (ER-Tracker Green, left), mitochondria (Mito-Tracker Green, center), and lysosomes (LysoTracker Green, right). Intracellular distribution was studied by fluorescence with appropriate selection of emission wavelengths. For each image, a profile of fluorescence intensity along the white arrow is shown. The green topographic profile corresponds to the emission of the tracker and the red profile to the photosensitizer emission.

Figure 5. Fluorescence micrographs of A549 cells co-incubated with F₂BMet and APF showing the red fluorescence from the photosensitizer (upper left) and the green fluorescence from fluorescein after illumination at 514 nm with the argon laser of the confocal microscope just on a single cell (upper right), the overlaid micrographs (lower right), and the bright-field image (lower left).

to 200 µm F₂BMet did not reveal any significant cytotoxicity. We selected $[F₂BMet]=5 \mu m$ for the phototoxicity studies with broadband irradiation because this dose leads to an accumulation of F₂BMet in A549 and S91-I3 cells comparable to that of related bacteriochlorins.^[7] The filtered halogen lamp has a relatively homogeneous power spectrum in the spectral region be-

from Refs. [7,19a], and on Photofrin from Ref. [41] with its P_OW at pH 7 from Ref. [42]. CIPOH was incubated at a concentration of 20 μ m, Photofrin at 17 μ m, and the bacteriochlorins at 5 μ m.

tween 630 and 800 nm, and is useful to compare the phototoxicity of different photosensitizers. Table 2 presents the lethal light dose required to kill 50 (LLD₅₀) or 90% (LLD₉₀) of the cells in the culture, respectively, calculated from data at different light doses. F_2 BMet is the most phototoxic photosensitizer.

Table 3 presents the photosensitizer concentrations required to kill 50 or 90% of A549, CT26, PC-3, and HT-29 cells, LD_{50} or LD_{90} , under laser-light doses of 1 and 6 J cm⁻². Additionally, we made a direct comparison between the dark cytotoxicities of F_2 BMet, *m*THPC, and Photofrin, and their phototoxicities under 1 J cm⁻² and 8 mW cm⁻² irradiation using CT26 and HT-29 cell lines. These cell lines were incubated with the maximum concentration of F_2 BMet, mTHPC, or Photofrin below the onset of their dark cytotoxicity and were irradiated with varying laserlight doses at 748, 652, and 633 nm, respectively. The low dark cytotoxicity of F₂BMet allows for the use of higher concentrations and the opposite is true for mTHPC. Figure 6 shows the resulting phototoxicities.

Biodistribution and pharmacokinetics

The biodistribution and pharmacokinetics of F_2 BMet were studied after intravenous (i.v.) injection in the tail vein of DBA/2 mice.

Groups of three or four animals were sacrificed at different time points and F_2 BMet was extracted from various tissues. Figure 7 shows the pharmacokinetics in blood, tumor, muscle, and skin. The largest concentrations of F_2 BMet, in terms of micrograms per gram of wet tissue, were observed in the liver, spleen, blood, and lungs, and are presented in the Supporting Information.

Photodynamic efficacy in vivo

The largest amounts of F_2 BMet in the tumor (T) relative to muscle (M) tissue were observed 24 (T/M=8) and 72 h (T/M= 16) post-i.v. administration. Thus, we made an exploratory study of PDT efficacy using DBA/2 mice with subcutaneously implanted S91 tumors for drug-to-light intervals (DLI) of 24 or 72 h. When a diameter of the tumor attained was approximately 5 mm, 2 mg kg⁻¹ of F_2 BMet was delivered in the tail vein, and after 24 or 72 h the tumors were illuminated with a light dose of 90 J cm^{-2} (diode laser at 750 nm, 90 mW). Figure 8 shows the time required for the tumors to attain the maximum diameter of 9.4 mm.

Table 3. Concentration of photosensitizers required to kill 50 or 90% of A549, PC-3, CT26, or HT-29 cells, in the dark or under a given laser-light (L) dose at 8 mW cm $^{-2}$.

Figure 6. Survival fractions of HT-29 and CT26 cells incubated with F₂BMet, mTHPC, or Photofrin below the onset of dark toxicity, as a function of the light dose.

Figure 7. Pharmacokinetics and biodistribution of F_2 BMet expressed as its concentration [μ gg⁻¹] in wet tissue for the blood, tumor, surrounding skin, and muscle as a function of the time after i.v. administration of 2 mg kg⁻¹ to DBA/2 mice with S91-I3 tumors; each point represents the mean \pm standard error of the mean (SEM) of three to four animals.

The illumination of the tumors with a single dose of 90 J cm $^{-2}$ led to the complete disappearance of the tumors in the following days. The protocol using $DLI=24$ h leads to large edema and to the formation of a necrotic scab in the tumor region and in its vicinity in the first day after the treatment. A milder tumor response occurred in the first days after treatment with the $DLI = 72$ h protocol. In this case, necrotic changes were observed 3–4 days after the illumination and covered only the tumor region, without significant damage to the skin. The 24 h protocol proved more effective in delaying tumor regrowth, with a median tumor growth delay of 50 days with respect to control. A 50 days median tumor growth delay in this exploratory study with 2 mg kg⁻¹ and 90 J cm⁻² at DLI $=$

24 h must be regarded as a very promising starting point for future work.

Discussion

Empirical structure–activity relationships

Sulfonamide halogenated bacteriochlorins can meet the physicochemical properties of photosensitizers that are critical to the success of PDT but, in spite of their similarities, they exhibit in vitro phototoxicities that differ by a factor of 50. For example, 6 J cm⁻² at 749 nm require

7.6 μ m of Cl₂BEt or 0.15 μ m of F₂BMet to kill 90% of the A549 cells. The PDT efficacy increases in the sequence ClBEt< $Cl₂BEt < FBMet < F₂BMet$, and is not anticipated by the conventional structure–activity factors: ε_{745} , Φ_{Δ} , Φ_{pd} , or P_{OW} . It is possible that small differences in these properties combine to yield the distinct phototoxicities systematically observed under drug- and light-dose-dependent experiments, but the most striking observation is that F₂BMet has the lowest Φ_{Λ} and the highest phototoxicity. The remarkable phototoxicity of F_2 BMet challenges the paradigm of PDT: the extent of type II reactions does explain relative phototoxicities and this highlights the relevance of type I reactions. Indeed, we have highlighted the role of charge-transfer interactions, $[15]$ and the focus of structure–activity relationships in PDT is shifting from correlations with $\log P_{\text{OW}}^{[43]}$ to the tuning of electronic properties.^[9e]

Figure 8. Kaplan–Meier plot of S91-I3 tumor regrowth in DBA/2 mice after PDT with 2 mg kg⁻¹ of F₂BMet i.v., followed by a light dose of 90 J cm⁻² at $DLI=24$ (solid line) or 72 h (dashed line), with respect to the control group (dotted line).

The pattern of median tumor-regrowth delays (in days) after PDT with bacteriochlorins, CIBOH $(27) <$ Cl₂BEt $(44) <$ F₂BMet (50), is similar to that of in vitro phototoxicity.^[16b,c] The biodistribution of F_2 BMet at times longer than 6 h post-i.v. administration is comparable to that of other bacteriochlorins of the same family, and the differences in the early time points are related to the use of intraperitoneal (i.p.) administration in the earlier studies.^[16b,c] The biodisponibility of F_2 BMet after i.v. administration of 2 mg kg^{-1} is also similar to that of Cl₂BEt after i.p. injection of 10 mg $\rm kg^{-1}$ (0.9 versus 1.0 $\rm \mu g \, kg^{-1}$ in the tumor). Thus, S91-I3 tumor-regrowth delays in DBA/2 mice after PDT reflect the relative in vivo PDT efficacy and strengthen the need for a finer rationale for in vitro phototoxicity.

Dynamics enhance PDT

The actual rate constant for the deactivation of the triplet state of the photosensitizer in the encounter complex with molecular oxygen can only be obtained after correction for diffusion [Eq. (5)]:^[44]

$$
k_{\rm D} = k_{\rm -diff} \ k_{\rm q} / (k_{\rm diff} \ - k_{\rm q}) \tag{5}
$$

in which $k_{\text{diff}} = k_{\text{diff}}/1$ m, but this is complicated by spin statistics. In the absence of charge-transfer interactions, $\frac{1}{9}k_{diff}$ should be used rather than k_{diff} , but in the presence of charge transfer both the singlet and triplet channels are active and $^{4}/_{9}$ k_{diff} should be used. The largest k_{q}/k_{diff} in ethanol was observed for FBMet and is between $\frac{1}{9}k_{\text{diff}}$ and $\frac{4}{9}k_{\text{diff}}$. Unfortunately, the correction for diffusion is dependent on the selection of the appropriate diffusion limit. Below we used a k_D value intermediate between these two limits in ethanol, $2.6 \times$ 10^9 M⁻¹ s⁻¹.

A large triplet deactivation rate constant (k_D) , manifested by $k_{\rm q}$ $>$ $\frac{1}{9}$ $k_{\rm diff}$, reveals the presence of significant charge transfer and should lead to a substantial fraction of oxygen-centered radicals. However, a large decomposition rate constant (k_d) , manifested by Φ_pd $>$ 10⁻⁵, should rapidly decompose the photosensitizer. Thus, the outcome of the ${sensitizer...O_2}$ interaction in the encounter complex determines the nature of the ROS and their throughput. Ideally a photosensitizer should combine fast quenching (efficient formation of oxygen-centered radicals) with slow photodecomposition (ability to endure many cycles of ROS generation). This is found in F2BMet.

Figure 9 shows that the relative PDT efficacy in vitro depends on the competition between ROS generation and degradation, k_D/k_d , for a constant rate of photon absorption (v_p). Appropriate offsets of the abscissa should be used for studies with different v_{p} , but this kinetic–activity relation is expected to be of great generality and provide a new rationale to guide the development of more efficient photosensitizers.

Figure 9. Top: reactive channels of the {sensitizer $\cdot\cdot\cdot O_2$ } interaction in the encounter complex. Bottom: Dependence of the light doses required to kill 90% of S91-I3 cells (LLD₉₀) or the photosensitizer doses required to kill 90% of PC3 cells on the balance between the reactive channels of halogenated sulfonamide bacteriochlorins.

Comparison with photosensitizers in clinical practice

 F_2 BMet has a much stronger absorption in the phototherapeutic window than Foscan (mTHPC for injection, approved for clinical use) and Photofrin, with a comparable Φ_{Λ} but additionally generates superoxide ion. The Φ_{pd} of F₂BMet in PBS/methanol (Φ_{pd} = 1.0 × 10⁻⁵) is smaller than that of Photofrin in PBS $(\Phi_{\rm pd} = 5.4 \times 10^{-5})$.^[45] The $\Phi_{\rm pd}$ of F₂BMet drops to 6.9×10⁻⁷ in aerated ethanol, which is also smaller than that of Foscan in methanol, $\Phi_{\rm pd} = 5 \times 10^{-6}$.^[45,46] F₂BMet is generally more photostable than the photosensitizers in clinical use and reacts faster with molecular oxygen, which is consistent with its ability to generate various oxygen-centered radicals. The preference for ER localization observed for F_2 BMet was also found for Foscan^[47] and Photofrin.^[48]

The comparison between these photosensitizers should be based on the ratio between dark cytotoxicity and phototoxicity, both defined for 50% of cell death, which was proposed as a therapeutic index (IP₅₀) of a photosensitizer [Eq. (6)]:^[49]

$$
IP_{50} = LD_{50dark}/LD_{50light} \tag{6}
$$

The measurement of the dark and light toxicities gives the following IP₅₀ values for CT26 cells: Photofrin (3.2), $mTHPC$ (81), and F_2 BMet (311). For HT-29 cells the corresponding values are Photofrin (2.4), $mTHPC$ (21), and F₂BMet (>540). The IP₅₀ of F₂BMet is the highest of these photosensitizers under the same light dose and fluence rate. The Supporting Information presents the cytotoxicity studies used to obtain the IP_{50} values.

The pharmacokinetics of F_2 BMet in mice exhibits a maximum concentration (C_{max}) in the blood shortly after i.v. administra-

tion and is well described by a two-compartment model with a distribution half-life of 1.1 h and a terminal half-life of 31 h. Plasma pharmacokinetics of Photofrin in human subjects follows a three-compartment model with half-lives of 2.08 min (distribution), 19.8 h, and 12.9 days.^[50] Clinical pharmacokinetics of Foscan is unusual because C_{max} is observed approximately 24 h post-i.v. injection and then the elimination half-life is 45.5 h.^[51] The elimination of F_2 BMet is faster than those of Photofrin and Foscan and should reduce the skin photosensitivity after the treatment, often cited as the major inconvenience of PDT. Interestingly, PDT was more effective with $DLI=24$ h than with $DLI=72$ h, which correlates better with the amount of photosensitizer in the vascular compartment than in the tumor.

Conclusion

A library of tetraphenylbacteriochlorins with fluorine or chlorine atoms in the ortho positions of the phenyl groups was explored to select the "ideal" PDT photosensitizer because such bacteriochlorins can be economically synthesized, $[10]$ exhibit a lower tendency to aggregate, $[52]$ combine strong absorptions in the phototherapeutic window with efficient formation of $long-lived$ triplet states,^[14a, 21b] bear electron-withdrawing groups that stabilize the macrocycle against oxidation,^[53] and provide steric protection.^[54] We found that the interaction between these bacteriochlorins and molecular oxygen led to superoxide ions and hydroxyl radicals in addition to singlet oxygen,^[9d, 15, 55] and the combined effects of these ROS were remarkably efficient in the destruction of tumor cells.^[7, 16c] However, empirical correlations with lipophilicity or with electronic factors were insufficient to drive the last stage of PDT photosensitizer discovery.

A new path to discovery was opened with the finding that the strength of the {sensitizer $\cdot \cdot \cdot O_2$ } interaction is revealed by the quenching rate constant. Values of $k_q \ge 2 \times 10^9$ M⁻¹ s⁻¹ in ethanol indicate the ability to generate superoxide ion in addition to singlet oxygen, especially in hydroxylic solvents where the nascent superoxide ion is stabilized by hydrogen bonding. However, k_q depends on E_{ox}^* and lowering E_{ox} increases the photodecomposition quantum yield, Φ_{nd} . The bleaching of the photosensitizer becomes a limiting factor of PDT efficacy when $\Phi_{\rm pd}$ > 10⁻⁵, which requires $E_{\rm ox}$ > 0.8 V versus SCE. The simultaneous fulfillment of the conditions $k_q \geq 2 \times 10^9$ M $^{-1}$ s $^{-1}$ in ethanol and $E_{\rm ex}$ > 0.8 V versus SCE should lead to photosensitizers that drive both type I and type II reactions without compromising photostability.

The dynamics of the interaction between the photosensitizer triplet state and oxygen determine both the nature of the ROS generated and the stability of the photosensitizer towards such ROS. F_2 BMet attains a delicate balance between a high degree of charge transfer to oxygen and an adequate resistance to oxidation. It is an example of how the dynamics of the interaction between light, a photosensitizer, and oxygen can be tuned to increase tissue damage. Interestingly, in 1904 the term "photodynamic" was used to distinguish PDT from the physicochemical processes occurring in the emulsions of pho-

tographic films.[1] Over one century later, dynamics provide a rationale to select the best photosensitizers for PDT.

Experimental Section

5,10,15,20-Tetrakis(2,6-difluoro-3-N-methylsulfamoylphenyl) porphyrin (F₂PMet)

A mixture of $F_2P^{[14a]}$ and chlorosulfonic acid (1:680) was added to a round-bottomed flask equipped with a magnetic stirrer. The mixture was kept at 110°C until the tetrachlorosulfonylated compound was observed by TLC. After cooling, dichloromethane was added, and the excess amount of acid was removed with a saturated solution of sodium bicarbonate in water. After evaporation the crude was redissolved in dichloromethane and a solution of methylamine in THF (2.0 m) was added. The reaction was kept at 20 \degree C until full consumption of the starting materials. Finally the solution was extracted with HCl (0.1m) and water. After chromatography with silica gel (dichloromethane/ethyl acetate), F_2 PMet was obtained in 70% yield. ¹H NMR (400 MHz, CDCl₃): $\delta = -2.84$ (s, 2H), 2.87-2.90 (m, 12H), 4.73 (m, 4H), 7.45–7.54 (m, 4H), 8.42–8.49 (m, 4H), 8.84 ppm (s, 8H); ¹⁹F NMR (376.5 MHz, CDCI₃): $\delta = -104.17$ to -104.11 (m, 4F); -98.54 to -98.49 ppm (m, 4F); HRMS (ESI-FIA-TOF): m/z calcd for $C_{48}H_{35}F_8N_8O_8S_4$: 1131.1327; found: 1131.1328 $[M+H^+]$; elemental analysis calcd (%) for $C_{48}H_{34}F_8N_8O_8S_4\cdot H_2O$: calcd C 50.17, H 3.16, N 9.75, S 11.16; found: C 50.47, H 3.18, N 9.39, S 10.94.

5,10,15,20-Tetrakis(2,6-difluoro-3-N-methylsulfamoylphenyl) bacteriochlorin (F₂BMet)

This bacteriochlorin was prepared on the multigram scale with our solvent-free method.^[13] A mixture of F_2 PMet and p-toluenosulfonylhydrazide (1:40) was ground in a Schlenk tube and then evacuated with a vacuum pump. Next, the reactor was heated at 140° C for 60 min, and then brought back to room temperature. After chromatography with silica gel (dichloromethane/ethyl acetate), F₂BMet was obtained in 85% yield. ¹H NMR (400 MHz, CDCl₃): δ = -1.38 (s, 2H), 2.77–2.84 (m, 12H), 4.06 (s, 8H), 4.65–4.71 (m, 4H), 7.39–7.43 (m, 4H), 8.00–8.03 (m, 4H), 8.24–8.29 ppm (m, 4H); 19F NMR $(376.5 \text{ MHz}, \text{ CDCl}_3): \delta = -105.09 \text{ to } -104.95 \text{ (m, 4F)}; -99.48 \text{ to }$ -99.37 ppm (m, 4F); HRMS (ESI-FIA-TOF): m/z calcd for $C_{48}H_{39}F_8N_8O_8S_4$: 1135.1640; found: 1135.1612 [M+H⁺]; elemental analysis calcd (%) for $C_{48}H_{34}F_8N_8O_8S_4 \cdot H_2O$: C 50.00, H 3.50, N 9.72, S 11.12; found: C 49.88, H 3.47, N 9.38, S 10.94.

Other porphyrin derivatives

The other photosensitizers employed in this study were available from previous studies or were synthesized according to the literature.^[10, 13] m THPP was synthesized by means of the nitrobenzene method, 56 and mTHPC was synthesized with our solvent-free method.^[13] Details are given in the Supporting Information.

Animals and tumor model

The animal model used for dark toxicity, biodistribution, and pharmacokinetic studies was the DBA mouse bearing the Cloudman S91-I3 melanoma. Following approval by the Jagiellonian University Committee for Ethics of Experiments on Animals (decision no. 89/2008 from 11 December 2008 and no. 11/2011, 23 February 2011), mice (20–30 g) from the Animal House of the Polish Academy of Science Medical Research Center (Warsaw, Poland) enrolled

in the experiments were kept on a standard laboratory diet with free access to drinking water. The S91 cells were cultured in vitro and after a subcutaneous inoculation of 1×10^6 cells into the right flank, tumors were induced in 100% of mice. The tumors grew exponentially and displayed only a little size scatter between animals.

Photodynamic therapy

S91-I3 tumors were grown in DBA/2 mice as described above. The treatment was initiated when the tumor attained at least 5 mm in one diameter in each animal. A dose of 2 mg kg⁻¹ of F_2 BMet was injected in the tail vein on the day the tumors reached the treatment size. At 24 or 72 h post-injection, the mice were anesthetized with ketamine and xylazine, and restrained in plastic holders, then treated with the Hamamatsu laser described above, at a fluence rate of 80–90 mW cm⁻² for 20 min. The mice (5–7 mice per group in three groups (not treated, treated with light, treated with light and photosensitizer) were checked daily. The tumors were measured using two radicular diameters L (length) and W (width) and the volumes were calculated using the formula $V = L \times W^2/2$.

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